

Description

As a dynamic system is considered in this case, in particular, any phenomenon whose time characteristic can be represented in a discrete form of the type

Also looked at, however, are systems with several (eg two) simultaneously detected time series x, y according to

$\alpha(t)$ is a set of characteristic system parameters, x is a state that generally forms a vector in a multidimensional state space, and y is a state displaced in time. The state space is created by variables that, for example, can be physical, chemical, biological, medical, geological, geometric, numerical and/or process engineering quantities.

The number of system variables that describe the system together with the dynamic response f corresponds to the

THE UNIVERSITY OF CHICAGO

Furthermore, this method is generally inapplicable in the case of parameters that vary with time. The analysis and modeling of dynamic signals are frequently hindered by the fact that the basic systems change with time in essential parameters. Examples are signals in medicine where an organ like the heart or the brain has many dynamic modes that alternate, or speech signals where the generating system, the mouth/pharynx region, apparently adopts different configurations in the course of time.

Another approach is known from the publication by K. Pawelzik, J. Kohlmorgen and K.-R. Mueller in "Neural Computation", vol. 8, 1996, p 340 ff, where data streams are segmented according to initially unknown system modes changing with time by simulation with several competing models. The models are preferably formed by neural networks, each characteristic of a dynamic response and competing to write the individual points of the data stream by predetermined training rules.

Segmentation according to K. Pawelzik et al., details of which are given below, allows allocation of segments to certain system dynamic responses or modes and leads to detection of the data stream as an operation with discrete "switching" between the modes. This description of the parameter dynamic response of complex systems is an advance in terms of accuracy and segmenting different system states compared to the above mentioned global modeling. Nevertheless, the transition between different system states cannot be described satisfactorily. In the analysis of real systems in particular, eg medical applications, it has been found that segmentation is limited to certain cases with mode differences that are as clear as possible and with low noise, and in general is unreliable when the generating system changes with time.

The object of the invention is to provide improved methods for detecting the modes of dynamic systems with transient system parameters, by which the restrictions of conventional methods can be overcome, and which in particular allow, with practicable effort and high reliability, automatic segmentation and identification of time series with an enhanced number of details.

The invention is based on the idea of comprehending transitions between different modes of a dynamic system as intermediate modes of the system that represent paired linear interpolations of the output and end modes of the transition. The observed dynamic systems tend to move gradually from one mode into another instead of switching abruptly between modes. The invention aims at identifying such transitions between different modes in signals and the modes.

Consequently, in a method for detecting the modes of dynamic systems, eg after switched segmentation of a time series of at least one of the system variables $x(t)$ of the system, drift segmentation is undertaken where, in each time segment in which the system transits from a first system mode s_i to a second system mode s_j , a succession of mixed prediction models g_i is detected given by a linear, paired superimposition of the prediction models $f_{i,j}$ of the two system modes $s_{i,j}$.

The subject of the invention is also a device for detecting a dynamic system with a large number of modes s_i , each with characteristic system parameters $\alpha(t)$. The device includes an arrangement for recording a time series of at least one of the system variables $x(t)$ of the system, an arrangement of switch segmentation for detecting a predetermined prediction model f_i for a system mode s_i in each time segment of a predetermined minimum length for the system variables $x(t)$, and an arrangement of drift segmentation with which a series of mixed prediction models g_i is detected in each time segment in which the system transits from a first system mode s_i to a second system mode s_j . The device according to the invention can also include an arrangement for setting interpolation and

[illegible]

Applications of the invention have shown that continuous transitions between system modes can be securely identified and that the fundamental dynamic responses can be described by the models with a precision that, in many cases, allows prediction of the system response. In many cases of non-stationary processes, the invention enables models to be identified that are suitable for control of the processes, these not being possible without considering the transience.

Fig. 1 Curves illustrating a first segmentation step of the method according to the invention,

Fig. 3 Curves of segmentation of blood regulating data after the method according to the invention, and

Fig. 4 Curves of segmentation of EEG data with the method according to the invention.

To begin with, details of the invention will be explained with reference to Fig. 1 and 2 and then examples of practical application. It will be clear to the skilled person that the invention is not restricted to the application examples but may also be used in other areas as exemplified further below.

(1) Detection of drift transitions in non-stationary time series

According to the invention, non-stationary time series are detected by a procedure in two steps: first suitable modeling and then so-called drift segmentation. The purpose of the modeling is to detect a predetermined prediction model for a system mode in each time segment of a predetermined minimum length for each system parameter. Here a conventional switch segmentation is preferred as known, for example, from the publication by K. Pawelzik et al. in "Neural Computation", vol. 8, 1996, p 340 ff. Modeling is also possible by another, in relation to the derived system information for switch segmentation, equivalent procedure that is matched to a concrete application, eg for known pure modes or boundary conditions.

The steps involved in switched and drift segmentation will now be explained in more detail. Where switched segmentation is concerned, the contents of the publication by K. Pawelzik et al. are completely introduced into the present specification by reference.



The functions f are derived as predictors (or prediction models, expert functions) from a set of networks with variable parameters by a suitable training program in which both the parameters of the networks and the segmentation are determined simultaneously. The term "network" is used here for all possible, suitable model functions, in other words preferably for neural networks but also for polynomials or linear function approximations for example. The optimum choice of a neural network is made according to the specific application. Preferably, networks with fast learning capability are used, eg RBF (radial basis function) networks of the type Moody-Darke.

Training involves maximizing the probability W that the set of networks would produce the time series $\{x_t\}$. This is training with competitive learning, as described in the publication "Introduction to the theory of neural computation" by J. Hertz et al. (Addison-Wesley Publishing Company, 1991), especially chapter 9 "Unsupervised competitive learning". The application-dependent implementation of such training can be derived from this publication. The training rule of competitive learning on the basis of the error occurring in learning can be represented according to

This training rule ensures that the learning speed (improvement of parameters) is highest for the functions f with the smallest distance from the target value y .

$$\begin{aligned} f_1(x) &= 4x(1-x) \text{ for } x \in [0, 1] \\ f_2(x) &= f_1(f_1(x)) \\ f_3(x) &= 2x \text{ for } x \in [0, 0.5] \text{ or} \\ &= 2(1-x) \text{ for } x \in [0.5, 1] \\ f_4(x) &= f_3(f_3(x)) \end{aligned}$$

f_1 is used first for the first 50 time increments with a start value of $x_0 = 0.5289$. Subsequently there is a transition (see (ii) for details) to mode f_2 , which becomes steady-state after increment 100 until increment 150. Accordingly, from increment 200 and increment 300 respectively, the mode f_3 and f_4 is each adopted for 50 increments. This is followed by a transition back to f_1 . Fig. 1a shows a section (increments 300 to 450) of the time response of the time series $\{x_t\}$ with $x_{t+1} = f(x_t)$.

The segmentation of the first 450 time increments with six predictors \underline{f}_i , $i = 1, \dots, 6$ (RBF networks of the type Moody-Darken) is shown in Fig. 1b. Training produces specialization of four of the predictors (6, 2, 4, 3) each to one of the four modes above. The steady-state regions are at the intervals [0, 50] and [400, 450] (f_1), [100, 150] (f_2), [200, 250] (f_3) and [300, 350] (f_4). The other two predictors (3, 5) have specialized to the transition regions between the modes. This shows the drawback of conventional switch segmentation, where, in the case of transitions, the particular time region is multiply subdivided without adequate description.

Instead of the so-called "hard competition" described here, where only one prediction model is optimized in a training

step (ie "winner takes all"), it is also possible to alter the degree of competition as part of "soft competition" training, as described in the publication by K. Pawelzik et al.

(ii) Step 2 (Drift Segmentation)

In the second step the transitions (socalled drifting, non-abrupt, sliding change) between the system modes are considered. In the invention, as an important requisite for drift segmentation, it was found that the transition from a first system mode is direct to a second system mode and not by way of a third system mode. Drifting between system modes is thus modeled by superimposition of - or paired linear interpolation between - precisely two modes. In this case mixed, possibly stepped intermediate modes appear, which are not system modes in their own right, ie pure, however.

A set of P pure system modes is considered, each represented by a network $k(s)$, $s \in P$, and a set of M mixed system modes, each represented by a linear superimposition of two networks $i(s)$ and $j(s)$, $s \in M$. The model network g_s for a given mode $s \in S$; $S = P \cup M$ is given by

$$g_s(\bar{x}_t) = \begin{cases} f_{k(s)}(\bar{x}_t) & \text{for } s \in P \\ a(s)f_{i(s)}(\bar{x}_t) + b(s)f_{j(s)}(\bar{x}_t) & \text{for } s \in M \end{cases} \quad (2)$$

In (2) \bar{x} is the vector $(x_t, x_{t-\tau}, \dots, x_{t-(m-1)\tau})$ of the time delay coordinates of the time series $\{x_t\}$ and $f_{i,j}$ are predictors determined according to the above switch segmentation. m is an imbedding dimension and τ the delay parameter of the imbedding. The imbedding dimension is the dimension of the phase space in

0000042 042000

which the system is considered and in which the models operate.

Two parameters a , b together with two network indexes i , j are characteristic of each mixed system mode. The number of mixed modes is limited to simplify the calculation effort. A finite number of values $a(s)$ are defined with $0 < a(s) < 1$ and $b(s) = 1 - a(s)$. For further simplification, equal intervals are selected between the values $a(s)$ according to

$$a_r = \frac{r}{R+1} \quad \text{with } r=1, \dots, R \quad (3)$$

R corresponds to the number of admissible intermediate modes and is also referred to as the resolution or graduation of the interpolation between the pure modes. The resolution R can assume any value, but it is selected sufficiently low as a function of application to achieve optimum system description (especially in heavily noise-corrupted operations) and practicable calculation times, especially in consideration of the switching rate given above. In practical applications (see below) it is possible for the resolution R to be selected manually by an operator or automatically by a control circuit as a function of an analysis result and comparison with a threshold value.

The total number of mixed modes is $|M| = R \cdot N \cdot (N-1) / 2$ for a given resolution R between two networks. In the above example the total number of mixed modes is thus $|M| = 896$ for $N = 8$ pure modes and resolution $R = 32$. The eight pure modes are added for determining the total number of system modes.

Drift segmentation now comprises the search for a segmentation with the pure and mixed system modes (a , b , R) that is optimized in terms of the prediction error of the modes of the

002240 24080550

The search for the segmentation with the smallest prediction error can be made by any suitable search or iteration technique. Preferable is a dynamic programming technique equivalent to the Viterbi algorithm for HM (hidden Markov) models. Details of this are to be found, for example, in the publication "A Tutorial on Hidden Markov Models and Selected Applications in Speech Recognition" of L. R. Rabiner in "Readings in Speech Recognition" (eds. A. Waibel et al., San Mateo, Morgan Kaufmann, 1990, pp 267-296). Where HM models are concerned, drift segmentation is the most probable mode sequence that could have generated the time series to be investigated. As an extra condition, the possibility of mode changes is restricted by the T function (see below).

The aim of the matching is the provision of an optimum sequence of networks or linear mixtures of them. A sequence is optimum when the so-called energy or cost function C^* of the prediction is minimized. The cost function C^* is composed of the sum of the square-law errors of the prediction and the cost functions of the mode transitions of the sequence.

Derivation of the cost function C^* between two points in time t_0 and t_{\max} is inductive, assuming initially a start cost function according to

$$C_s(t_0) = \varepsilon_s(t_0) \quad (4)$$

where

$$\varepsilon_s(t) = \left(x_t - g_s(\bar{x}_{t-1}) \right)^2 \quad (5)$$

is the square-law error of the prediction of the pure or mixed modes g .

For the induction step from $t - 1$ to t , the cost function is computed according to equ. (6) for all $s \in S$

$$C_s(t) = \varepsilon_s + \min_{s \in S} \{C_s(t-1) + T(\hat{s}, s)\}, \quad t = t_0 + 1, \dots, t_{\max} \quad (10)$$

where $T(\hat{s}, s)$ is the cost function of the transition from a mode \hat{s} to a mode s .

The optimum (minimum) cost function C^* is then

$$C^* = \min_{s \in S} \{C_s(t_{\max})\} \quad (11)$$

In the HM models the function T corresponds to the transition probabilities and can be selected as suitable for the application. It is possible, for example, to allow abrupt switching transitions and sliding drift between two networks and to eliminate all other transitions by $T = \infty$.

Drift segmentation can be followed by an extra step of reducing the number of networks used for modeling, this being explained below.

The result of drift segmentation in the case of the chaotic time series $\{x_t\}$ with four modes that is explained above with reference to Fig. 1 is described in what follows with reference to Fig. 2. Drift segmentation comprises the search for a response $a(t)$ that produces a special path between the pure modes for which the prediction error of the entire time series is optimized.

$$\begin{aligned} f(\bar{x}_t) &= (1 - a(t))f_1(\bar{x}_t) + a(t)f_2(\bar{x}_t) \\ \text{with} \quad & \\ a(t) &= \frac{t - t_a}{t_b - t_a} \quad t_a = 50, t_b = 100 \end{aligned} \quad (12)$$

Corresponding transitions occur for 50 increments in each case after the 150th, 250th and 350th increment.

Fig. 2 shows the occupancy of the particular modes according to the determined networks as a function of time (time increments [1200, 2400]). For the sake of clarity the transition or drift regions are presented, according to their time limits and outset or end modes, in frames in which the particular drift between the modes is dotted. Fig. 2a shows, for resolution $R = 32$ (see equation 3), transitions as for the time increments 1350 through 1400 between networks 2 and 4. The transitions are linear, as can be expected from equation (8). Lower resolution of $R = 3$ produces the segmentation shown in Fig. 2b. Unlike the linear drift, here the dotted transitions are stepped. Nevertheless, this presentation at lower resolution is still an adequate description of the dynamic response of the system, as a comparison between the timing of the modes and the drift demonstrates.

(2) Application examples for detecting drift transitions

(i) Blood cell regulation in the human body

Blood cell regulation in the human body is a highly dimensional, chaotic system that can be described by the following Mackey-Glass delay differential equation (refer also to the above publication by J. Hertz et al.):

$$\frac{dx(t)}{dt} = -0.1x(t) + \frac{0.2x(t - t_d)}{1 + x(t - t_d)^{10}} \quad (13)$$

According to the invention, time series of physiological parameters that are characteristic of the set of red blood cells can be segmented as a function of application. The functionality of the segmentation is explained and exemplified below.

$$a(t) = \exp\left(\frac{-4t}{100}\right), \quad t = 1, \dots, 100 \quad (14)$$

Nevertheless, two networks have specialized on one mode (2, 3 \Rightarrow mode A, 5, 6 \Rightarrow mode B), respectively. In such a situation the invention provides for the extra step of reducing the number of networks used for modeling.

The reduction step comprises sequential reduction of the number of networks, combined in each case with determination of the mean prediction error. Reduction (withdrawal of redundant networks) is ended if continuing reduction of the number of networks means a significant increase in prediction error. Fig. 3c shows the result of such reduction. The root

Adequate model networks are obtained by computing the RMSE value for each network combination with a reduced number of networks. The network combination with the smallest RMSE comprises the sought model networks or predictors. Fig. 3d shows drift segmentation after the reduction step. The remaining predictors 2 and 5 describe the system in its entirety.

A further application for the invention is to be found in the analysis of physiological data that are characteristic of the sleeping and waking modes of humans. Time series of EEG data, for example, can be segmented as a basis for subsequent procedures to detect sleep disorders.

Fig. 4a shows by comparison the results of a conventional switch segmentation (top), a drift segmentation (center) and a "manual" segmentation (bottom) by a medical specialist (sleep researcher) based on empirical values in the example of an afternoon sleep by a healthy person. The switch and drift segmentations are produced with eight networks (net1 through net8) on single-channel EEG data $x(t)$ (Fig. 4b). In Fig. 4a, as in Fig. 2, frames are drawn for the sake of clarity to illustrate between which networks there is interpolation in the drift modes. The dotted line inside the frames indicates the actual response in each case. Manual segmentation is based on the observation of physiological signals (eg EEG, EOG, ECG,

Switch segmentation shows a comparatively undifferentiated picture that is only roughly consistent with the other observations. Thus a predormition phase occurs in all three cases at $t \approx 7000$. Drift segmentation produces several drift transitions, however, that represent additional details of sleep behavior. The "manually" observed beginning of sleep at $t \approx 4000$ is represented by an exponential drift transition from net7 (wake mode predictor) to net4 (sleeping mode predictor). Awakening begins at $t \approx 9000$ through a slight drift back to net7, which is maintained until the "manually" determined waking point $t \approx 9500$ is reached. In this situation there is a sudden change of the weighting factor, so that net7 takes on greater weighting. After $t \approx 9800$ (eyes open) there is a mixture of the two wake mode predictors net7 and net2.

Fig. 4a shows that detailed segmentations can be automatically produced by the method according to the invention that to date were only possible by observing complex features on the basis of broad experience and intuition. This advantage can be made use of not only in medicine but also in other areas where large amounts of data occur when describing complex dynamic systems. Such areas are physical, chemical and/or biological process engineering, geology, meteorology, climatology, speech detection.

Methods according to the invention present the following advantages. The observed system can be highly dimensional (ten

Use of the invention for prediction or control of a system works as follows. First, as described above, the actual state of the system is detected from preceding observation and knowledge of the current modes, this possibly being a mixture according to the result of drift segmentation. The actual state corresponds to a dynamic system f . Prediction means that the system f is applied to the momentary state x , resulting in the prediction for the state y that directly follows. Control means that the deviation from a setpoint state is determined from the actual state, and that an appropriate control strategy is derived from the deviation.

The advantage of prediction and control is that in complex systems (eg detecting chemical reactions in a reactor), possibly only allowing measurement of a few variables, which themselves do not permit direct conclusions about the state of the system and any mixed states that exist because of ambiguities or system-immanent delays, detailed information about the system can nevertheless be derived. Thus, in the example with a chemical reaction, an optimum control strategy, comprising the dosing of certain coreactants, can be derived from detection, according to the invention, of the macroscopic, thermodynamic state variables for instance.